

# A low cost sEMG controlled robotic hand for amputees

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## Abstract

Amputees who have undergone a wrist disarticulation often use an artificial hand or hook prosthesis to regain part of the lost function. However, advanced robotic prostheses remain economically out of reach of many patients. This project proves that a low cost surface EMG controlled prosthetic hand can be built and be fully operational. A special EMG sensor with dry electrodes was developed, together with a hand mechanism actuated by servo-motors. Force sensitive resistors were placed on the palm of the artificial hand to provide some level of feedback and allow for soft gripping. The whole machine is controlled with an Arduino Mega 2560 board clone. The cost of materials is less than \$200.

## Executive Summary

A robotic prosthetic hand was constructed. It utilizes surface EMG from the user's forearm as its control signals. Each finger can be extended and flexed independently. A force feedback mode allows the hand to operate in a "soft-grip" mode.

## Introduction

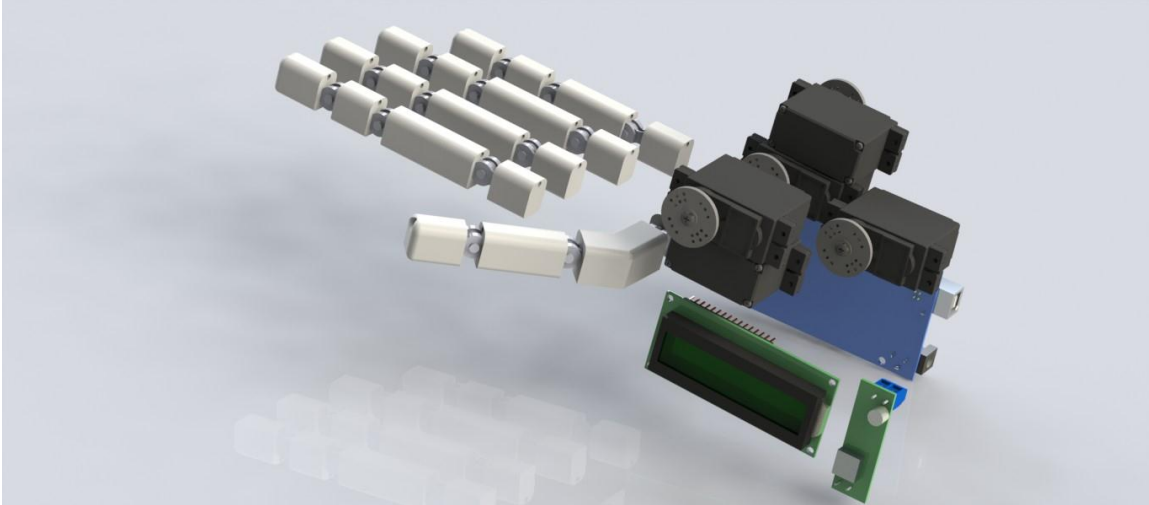
This project explores the possibility of constructing a low-cost prosthetic hand for amputees that can be controlled with surface electromyography. Surface electromyography (sEMG) is a sensing technique that allows the capture of action potentials of muscles during activation. Most advanced prosthetic hands found in the market provide great capabilities but come at a steep cost (reaching up to \$35,000 for the bebionic hand [1]) making it virtually inaccessible to a large number of people who could benefit from it, especially in underdeveloped countries.

The robotic hand was constructed using servo-motors for actuation, and custom-made EMG sensors. Additional components include an LCD screen, two buttons, and two force-sensitive resistors (FSRs). After three months of development, the machine operates properly.

## Integrated system

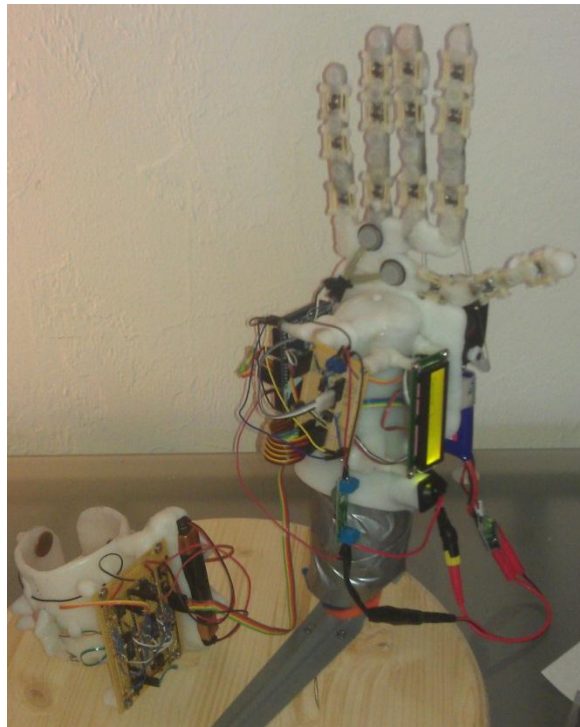
### CAD model overview

The use of Solidworks to model and display several components of the prosthetic assembly facilitated some design choices, e.g. placement of the servomotors in their final configurations. This saved time and money since it became possible to verify if there was interference between the different components.



**Figure 1. Rendering of CAD assembly**

Even though CAD modeling was useful, the design was not based on CAD drawings. The design was driven almost completely by the manufacturing capabilities at my disposal.



**Figure 2. Picture of the completed robot**

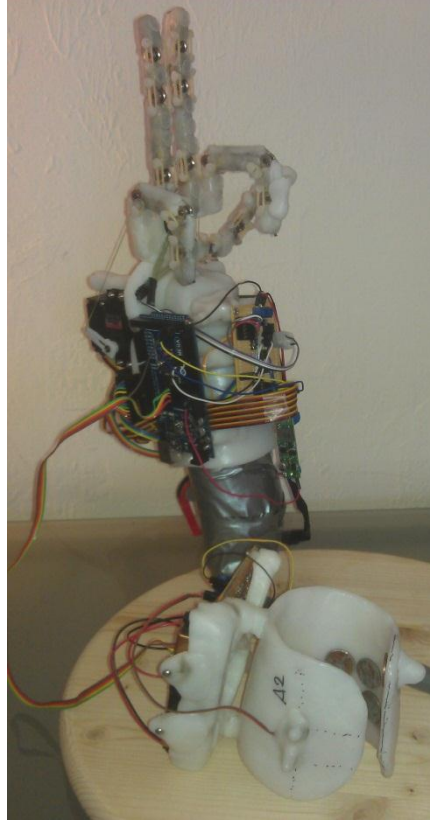


Figure 3. Picture of the completed robot.

## Mobile Platform

### Hand mechanics

Each of the fingers is being flexed by several elastic bands crossing each joint. By selecting a number of elastic bands for each joint it is possible to create roughly equal moments across all the joints in a finger. When a force is applied at the tip of the finger, tangential to the fingertip causing extension, the finger assumes a shape with roughly equal angles in all its joints. This creates a smooth natural-looking opening and closing motion.

### Attachments to arm

The prosthetic's platform contains a socket for the amputee's stump. It was molded according to my arm geometry. However, it is not design to fit anyone in particular. Since the platform is for demonstration purposes only, fit and comfort are not issues.

### Materials used

The body of the prosthetic limb is made primarily out of plastic. The commercial name of the plastic is Instamorph. Similar to other moldable polyester thermoplastics, it is non-toxic, biodegradable, and lightweight. It becomes moldable at 60°C.

The joints of the fingers are made out of a bicycle chain (steel). The fingers are passively flexed by orthodontic elastic bands made of latex. The strings that serve as tendons are made of high strength nylon fishing line.

## Actuation

Servo-motors:

Tests performed:

- Torque test extending index finger. This test verified that the servo-motor selected could extend a finger under the experimental conditions.
- Opening and closing of all fingers at once.

Selection criteria: Cost, torque, speed, size, and availability.

Performance: Sufficient. It takes approximately one second to extend a finger under the maximally pre-loaded condition.

## Sensors

### Surface EMG sensors

#### Principles of operation

There is extensive documentation in the literature regarding EMG sensing and measurement, along with techniques for post-processing EMG data. The following is a brief introduction to EMG as stated by [2]

“A surface electromyogram (sEMG) signal is the electrical manifestation of the neuromuscular activity and is recorded non-invasively from the surface of the skin ([Hogan and Mann, 1980] and [deLuca, 1979]). The sEMG signal has been extensively used for estimation and interpretation of the neural drive to muscles (Merletti et al., 1999), extraction of a voluntary command signal for control of prosthetic devices for individuals suffering from limb amputation ([Heftner and Jaros, 1988], [Park and Meek, 1995] and [Huang et al., 2005]), and in biofeedback experiments in which the subjects learn to change patterns of voluntary muscle contraction ([Ince et al., 1984], [Radhakrishnan et al., 2008], [Bloom et al., 2010] and [Nazarpour et al., 2012]) “

#### Rationale behind EMG sensor use

The muscles that control hand motion are located in the forearm. Since a hand amputees may still retains these forearm muscles, these remain as the most obvious source of control signals for use in a prosthetic. EMG signals can be obtained via surface electrodes or fine-wire electrodes. The fine-wire provides signals from within the muscle. They are able to reach deep muscles and aren't prone to skin motion artifact, or muscle motion artifact. However, these probes compromise the safety (infection) and comfort (pinching) of the user, and hence were not considered for this project. In the other hand, surface electrodes can be made cheaply, and used safely.

## EMG sensor design

The EMG sensor was designed to be compact, inexpensive, and easy to attach. The electronics are shown in Figure 4 and were based on the sensor design published by Advancer Technologies [3]. Two main changes were implemented. The original sensor performs rectification and low-pass filtering in the circuitry. This sensor instead uses the third op-amp to amplify the signal and also bias it. The rectification and low-pass filtering is done in the software via calibration and moving average functions.

The mount was made by molding a sheet of plastic to my forearm geometry. The electrodes were made out of pennies. I used a rotating tool to flatten the faces, therefore removing dirt and oxides. Wood screws were then glued to the pennies, and some solder was applied to guarantee conductivity. The penny/screw assemblies were then inserted into the plastic mount. The screws were then soldered to wires, and covered in more plastic.

The mount for the PCB and batteries was molded out of plastic, and attached to the arm mount in two places, such that the arm mount may retain its compliance. This design allows the arm mount to clamp to the forearm and press the electrodes to the skin. Having all the electrodes, including ground, attached to a single object makes the sensor easy to use and adjust.

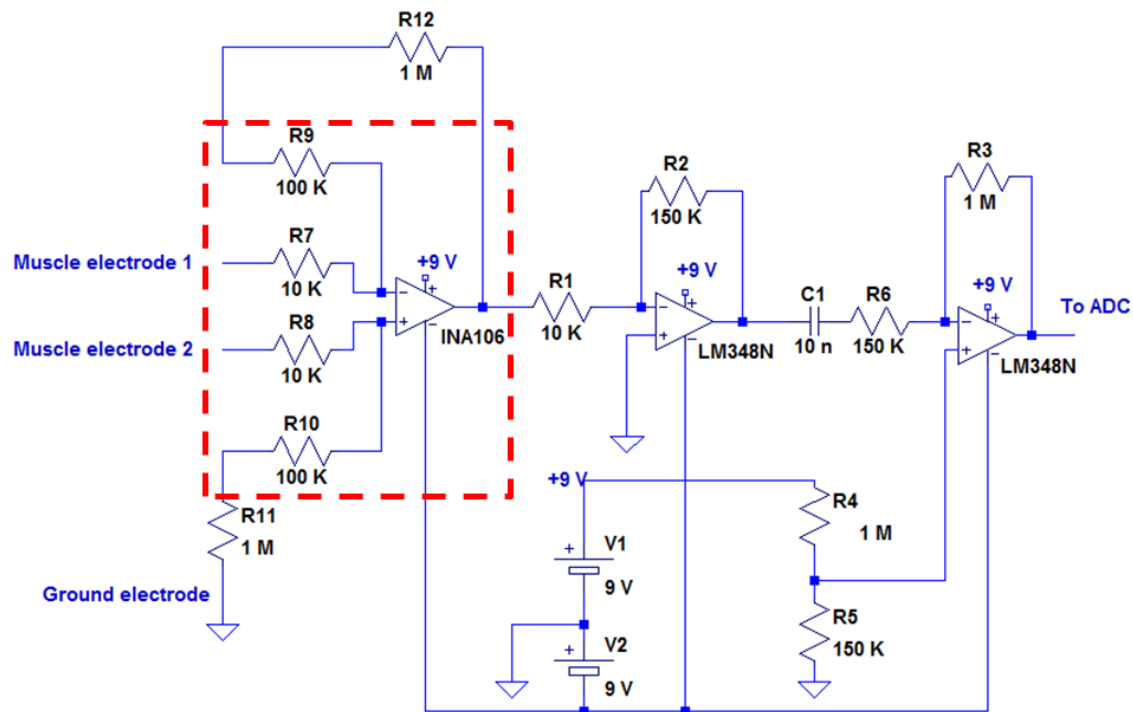


Figure 4. EMG sensor electronics design. The red box indicates an IC component. All the resistors in the red box are embedded on the INA106 chip.

### Instrumentation necessary

In order to verify the behavior of the sensor, I used a program that turns a laptop's sound card into an oscilloscope. This proved crucial since it allowed me to observe and capture sEGM signals at home. I later used the Arduino board itself and 3<sup>rd</sup> party software (Processing, Parallax DAQ, and Excel) to plot the analog signal.

### EMG signal processing

The flowchart in Figure 5 shows the sequence of EMG signal processing. The initial part is taken care of in hardware. After the signal is amplified and biased in hardware, the ADC can read it and so the signal processing now is done in the software. The signal is demeaned and rectified. A moving average of 100 samples is calculated and finally, the signal is transformed by squaring it and scaling it. The last step is meant to make the low signal values due to noise, even smaller, and the larger meaningful signal even larger.

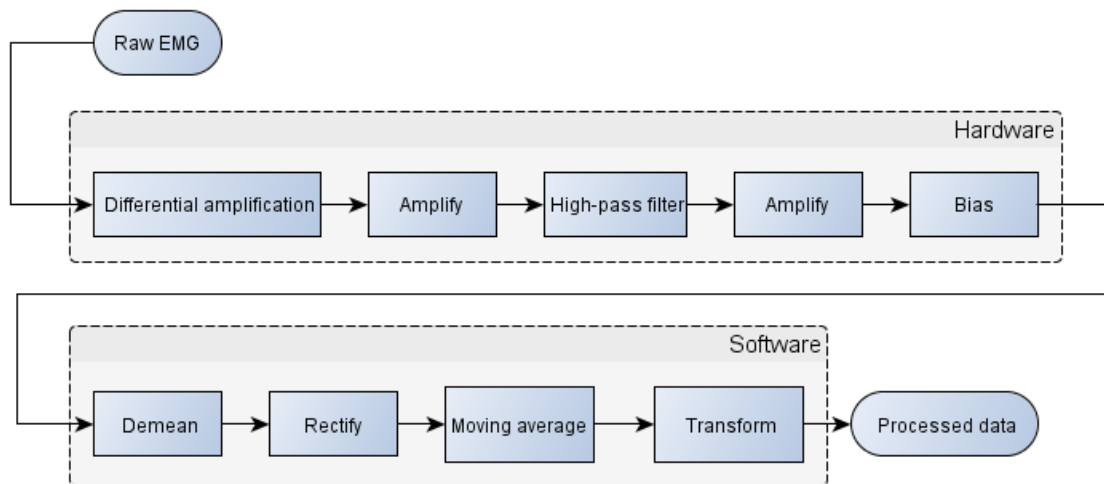


Figure 5. Flowchart describing sequence of EMG processing

### Force sensors

In order to detect when an object was being held gently, force sensitive resistors (FSRs) were added to the platform. They were located in the “palm” of the prosthetic hand. Small sticky rubbery pads were attached to these sensors in order to increase the likeliness of contact. They were placed in a voltage divider configuration.

### Behaviors

A summary of the behavior is shown in Figure 6.



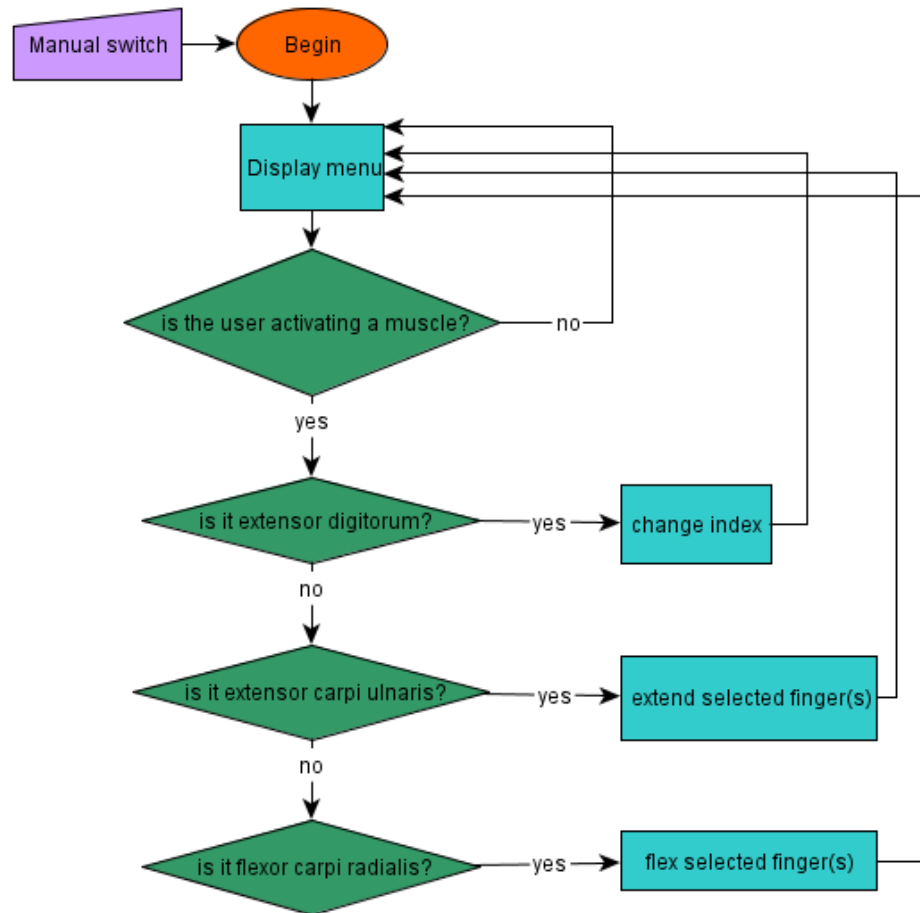


Figure 6. Summary of robot behavior

The LCD will be displaying information at all times. The data shown in the LCD will change depending on the menu option selected. The menu option is toggled by pressing button 1 on the main board.

The robot has two modes of operation:

- 1) Force-feedback enabled: Flexes selected finger(s) by slowly performing a servo sweep. It will stop the sweep before reaching the closed position if any of the force sensors surpass a pre-establish threshold.
- 2) Force-feedback disabled: Flexes selected finger(s) in a swift motion regardless of force sensor feedback.

### How to control the robot

Contracting different muscles will perform different actions. Table 1, shows the control strategies programmed.

**Table 1. Table showing correspondence between muscle activated, motion, and robot action.**

<b>Muscle</b>	<b>Motion by human</b>	<b>Action by robot</b>
Flexor carpi radialis	Flexing wrist	Closing
Extensor carpi ulnaris	Extending wrist	Opening
Extensor digitorum	Extending fingers, flexing fingers	Change selected finger(s)

## Cost

The total cost of all parts used in the robot was below \$200 as shown in Table 2. Estimated cost of all parts. Some parts were obtained for free as samples.

**Table 2. Estimated cost of all parts.**

<b>Part</b>	<b>Number of parts</b>	<b>Cost per part (USD)</b>	<b>Total cost (USD)</b>
Arduino Mega 2560 clone	1	25	25
Switching voltage regulator	1	25	25
Plastic	1	30	30
Bicycle chain	1	7	7
Orthodontic elastic band set	1	5	5
LCD screen	10	1	10
PCB board	2	2.5	5
Differential amplifier	3	~ 5	15
Op-amp	2	2	4
LiPo battery	1	7	7
FSR	2	5	10
Servo-motor (Hitec hs322-hd)	5	10	50
High strength nylon string	-	-	~ 0
9 V battery	2	~ 3	~ 6
<b>TOTAL</b>	-	-	<b>~ 199</b>

## Code structure

The complete code is provided in the documentation section. However, a flow chart showing the structure of the code is provided below, in Figure 7.

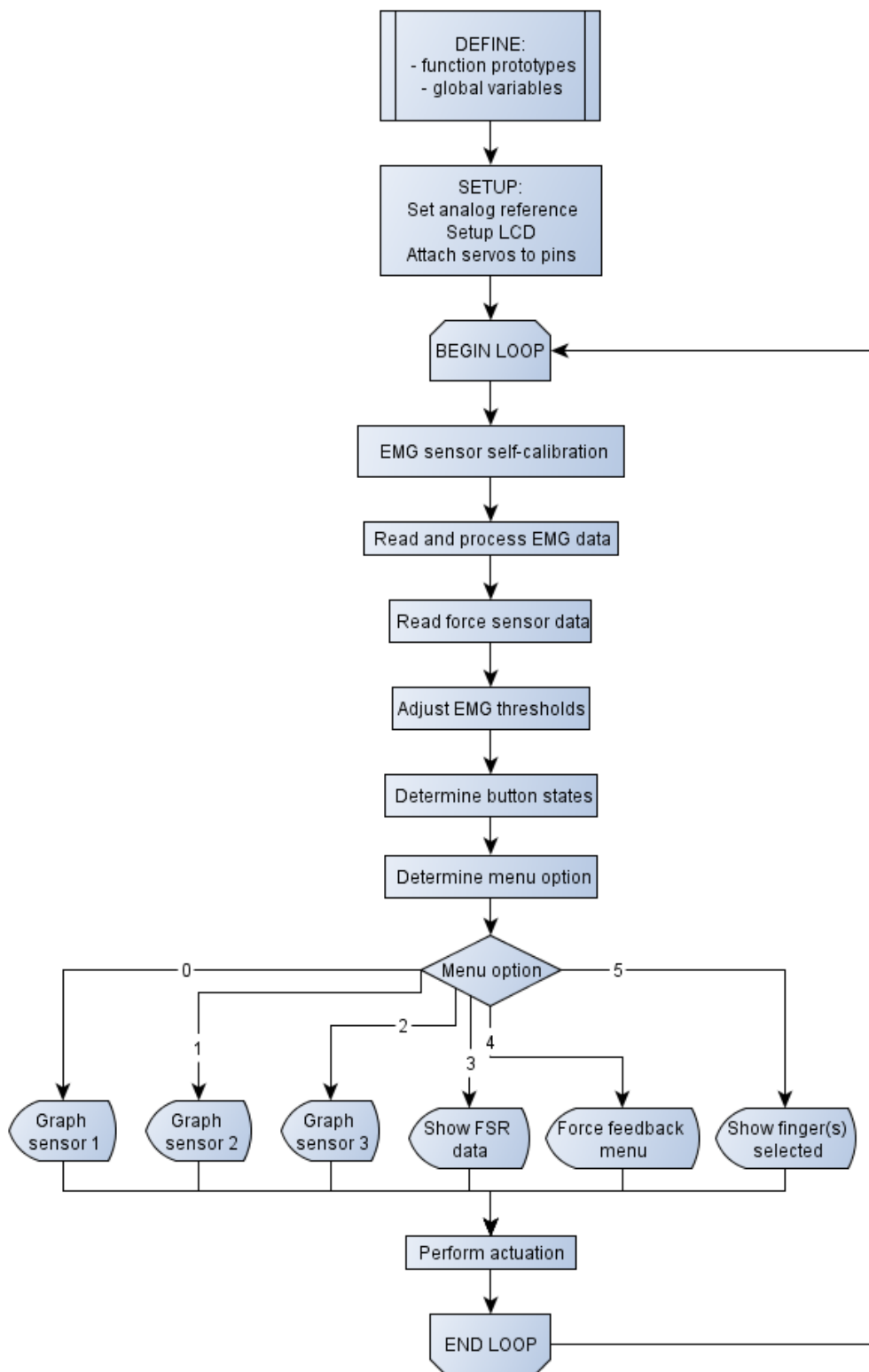


Figure 7. Code overview

## Conclusion

A working prototype was obtained. It is responsive to muscle activations and allows for grasping of different objects. Thus, it has been shown that the technology to create a low-cost sEMG-controlled robotic hand prosthesis is readily available.

## Documentation

The following is the final version of the code:

```
#include <LiquidCrystal.h>
#include <LcdBarGraph.h>
#include <Servo.h>

// function prototypes
int process_EMG(int rawEMG, int signal[], int &smin);
void calibrate();
void setButton1State();
void setButton2State();
void graphSensor(int sensorNumber);
void hand_open();
void hand_close();
void set_threshold(int smin, int &st);
void set_threshold_index(int smin, int &st);
void reg_open();
void reg_close();
void forceFB_close();
void sweep_servo(Servo &myServo, int flex_angle, int ext_angle);
void sweep_ALL_servos();

// Servos
Servo finger1; // thumb, PWM 10
Servo finger2; // index, PWM 12
Servo finger3; // middle, PWM 13
Servo finger4; // ring, PWM 9
Servo finger5; // pinky, PWM 11
int flex_a1 = 10;
int flex_a2 = 0;
int flex_a3 = 180;
int flex_a4 = 0;
int flex_a5 = 180;
int ext_a1 = 180;
int ext_a2 = 130;
int ext_a3 = 25;
int ext_a4 = 115;
int ext_a5 = 70;
```

```

int PosSweepDelay = 15; // 15ms to delay each position for sweeping a servo
long timeOfLastSweep = 0;
int timeBetweenSweeps = 1000; // 1 second "delay" between sweeps

// LCD setup
byte lcdNumCols = 16; // -- number of columns in the LCD
LiquidCrystal lcd(7, 6, 5, 4, 3, 2); // -- creating LCD instance
LcdBarGraph lbg(&lcd, lcdNumCols); // -- creating
const int graphMax = 100; // maximum value to graph

// calibration
int calibSignal = 0; // signal to gather sensor 1 data and calibrate
int calibSize = 300; // how many data points are used to obtain average
float calibSum = 0; // sum of all measurements
int calibCount = 0; // how many times you have added measurements
int cal = 428; // calibration value

// EMG sensors
const int filterSize = 100;
int signal_1[filterSize] = {
  0};
int signal_2[filterSize] = {
  0};
int signal_3[filterSize] = {
  0};
int sensorVal_1 = 0;
int sensorVal_2 = 0;
int sensorVal_3 = 0;
long start = 0;
int previous_index = 0;
int index = 0; // 0: whole hand, 1: thumb, ..., 5: pinky
long timeOfLastToggle = 0;
long indexToggleWait = 1000; // wait 200ms before each toggle
boolean lock_index = 0; // 0 is unlocked
long timeOfLock = 0; // time when finger motion was blocked
int lockDuration = 500; // delay required going from one configuration to another

// FSR sensors
int FSR1=0;
int FSR2= 0;
boolean FFB_state = 0; // start force feedback in the OFF state
const int FSR_val = 350; // FSR threshold for stopping gesture
long FSR_timeOfLock = 0;
const int FSR_printDelay = 100;

// threshold setting

```

```

int s1t = 80; //sensor 1 threshold
int s2t = 80; //sensor 2 threshold
int s3t = 80; //sensor 3 threshold
int s1min; // moving minimum for sensor 1
int s2min; // moving minimum for sensor 2
int s3min; // moving minimum for sensor 3

// buttons
const int button1Pin = 52; // the number of the pushbutton 1 pin
const int button2Pin = 53; // the number of the pushbutton 2 pin
int button1State; // the current reading from the input pin
int button2State; // the current reading from the input pin
int lastButton1State = LOW; // the previous reading from the input pin
int lastButton2State = LOW; // the previous reading from the input pin
long lastDebounceTime1 = 0; // the last time the output pin was toggled
long lastDebounceTime2 = 0; // the last time the output pin was toggled
long debounceDelay = 50; // the debounce time; increase if the output flickers
long timeDelay = 400;
long lastTimeOn1 = 0;
long lastTimeOn2 = 0;

// LCD menu
int option = 0;

void setup() {
  analogReference(INTERNAL2V56);
  // -- initializing the LCD
  lcd.begin(2, lcdNumCols);
  lcd.clear();
  delay(100);
  pinMode(8, OUTPUT);
  analogWrite(8, 80); // pin for contrast control
  //Serial.begin(9600); // initialize the serial communication:
  finger1.attach(10); // attaches pins to servos
  finger2.attach(12);
  finger3.attach(13);
  finger4.attach(9);
  finger5.attach(11);
}

void loop() {
  //Serial.println(millis()-start);
  if (millis()-start > 1)
  {
    start = millis();
    calibrate(); // self calibration
  }
}

```

```

sensorVal_1 = process_EMG(analogRead(A0),signal_1, s1min); // process sensor 1
sensorVal_2 = process_EMG(analogRead(A1),signal_2, s2min); // process sensor 2
sensorVal_3 = process_EMG(analogRead(A2),signal_3, s3min); // process sensor 3
FSR1 = analogRead(A8);
FSR2 = analogRead(A9);
set_threshold(s1min, s1t);
set_threshold_index(s2min, s2t);
set_threshold(s3min, s3t);

setButton1State(); // checks the state of button 1. Pressing returns a 1 for one cycle
setButton2State(); // checks the state of button 2

if (option < 6)
{
  if (button1State)
  {
    option++;
    lcd.clear();
  }
}
else {
  option = 0;
}
// display menu options
switch(option)
{
case 0:
  graphSensor(1);
  break;
case 1:
  graphSensor(2);
  break;
case 2:
  graphSensor(3);
  break;
case 3:
  if (millis()-FSR_timeOfLock > FSR_printDelay)
  {
    lcd.clear();
    lcd.setCursor(0, 0);
    lcd.print("FSR 1: ");
    lcd.print(FSR1);
    lcd.setCursor(0,1);
    lcd.print("FSR 2: ");
    lcd.print(FSR2);
    FSR_timeOfLock = millis();
  }
}

```

```
}
  break;
case 4:
  lcd.setCursor(0,0);
  lcd.print("Force feedback");
  lcd.setCursor(0,1);
  lcd.print("mode: ");
  if (FFB_state == 1)
  {
    lcd.print("ON");
  }
  else
  {
    lcd.print("OFF");
  }
  break;
case 5:
  if (previous_index != index){
    lcd.clear();
    previous_index = index;
  }
  lcd.setCursor(0,0);
  lcd.print("Index: ");
  lcd.print(index);
  lcd.setCursor(0,1);
  switch(index)
  {
  case 0:
    lcd.print("All fingers");
    break;
  case 1:
    lcd.print("Thumb finger");
    break;
  case 2:
    lcd.print("Index finger");
    break;
  case 3:
    lcd.print("Middle finger");
    break;
  case 4:
    lcd.print("Ring finger");
    break;
  case 5:
    lcd.print("Pinky finger");
    break;
  }
```



```

    break;
}

if (option == 4) // force feedback screen
{
    if (button2State)
    {
        lcd.clear();
        if (FFB_state) // toggle between on and off state
        {
            FFB_state = 0;
        }
        else
        {
            FFB_state = 1;
        }
    }
}

//after menu options are displayed. Timing of menu option change
if (sensorVal_2 > s2t && (millis()-timeOfLastToggle) > indexToggleWait) // finger
extensor
{
    previous_index = index;
    if (index < 5) {
        index++;
    }
    else
    {
        index = 0;
    }
    timeOfLastToggle = millis();
}
//
if (sensorVal_1 > s1t && (millis()-timeOfLock) > lockDuration) // wrist extensor
{
    lock_index = 1;
    timeOfLock = millis();
    reg_open(); // opening
}
if (sensorVal_3 > s3t && (millis()-timeOfLock) > lockDuration) // wrist flexor
{
    lock_index = 1;
    timeOfLock = millis();
    if (FFB_state == 0)
    {

```

```

    reg_close(); // closing blind
  }
  else
  {
    if (millis()-timeOfLastSweep > timeBetweenSweeps)
      forceFB_close(); // sweep servos to close while sensing for force
    }
  }
}
}

int process_EMG(int rawEMG, int signal[], int &smin) // returns sensorVal but changes
smin
{
  smin = 10000; // initialize smin
  int rectEMG = abs(rawEMG-cal); // demean and rectify
  for (int i = 0; i < filterSize-1; i++) {
    signal[i] = signal[i+1];
  } // shift signal array by one
  signal[filterSize-1] = rectEMG; // add last entry to signal array

  int total = 0;
  for(int i = 0; i < filterSize; i++) {
    total += signal[i];
    if (signal[i] < smin)
    {
      smin = signal[i];
    }
  }
  int sensorVal = (total / filterSize)^2/10; // get average and transform
  return sensorVal; // return transformed moving average
}

void calibrate()
{
  calibSignal = analogRead(A0);
  calibSum += calibSignal;
  calibCount++;
  if (calibCount == calibSize-1)
  {
    cal = calibSum/calibSize;
    calibSum = 0;
    calibCount = 0;
  }
}
}

```

```
void setButton1State()
{
  if ((millis() - lastTimeOn1) < timeDelay && lastButton1State == 1)
  {
    button1State = 0;
  }
  else
  {
    int reading = digitalRead(button1Pin);
    // If the switch changed, due to noise or pressing:
    if (reading != lastButton1State)
    {
      // reset the debouncing timer
      lastDebounceTime1 = millis();
    }

    if ((millis() - lastDebounceTime1) > debounceDelay) {
      // whatever the reading is at, it's been there for longer
      // than the debounce delay, so take it as the actual current state:
      button1State = reading;
    }
    // save the reading. Next time through the loop,
    // it'll be the lastButtonState:
    lastButton1State = reading;
    if (button1State == 1)
    {
      lastTimeOn1 = millis();
    }
  }
}

void setButton2State()
{
  if ((millis() - lastTimeOn2) < timeDelay && lastButton2State == 1)
  {
    button2State = 0;
  }
  else
  {
    int reading = digitalRead(button2Pin);
    // If the switch changed, due to noise or pressing:
    if (reading != lastButton2State)
    {
      // reset the debouncing timer
      lastDebounceTime2 = millis();
    }
  }
}
```

```
}

if ((millis() - lastDebounceTime2) > debounceDelay) {
  // whatever the reading is at, it's been there for longer
  // than the debounce delay, so take it as the actual current state:
  button2State = reading;
}
// save the reading. Next time through the loop,
// it'll be the lastButtonState:
lastButton2State = reading;
if (button2State == 1)
{
  lastTimeOn2 = millis();
}
}
}

void graphSensor(int sensorNumber)
{
  switch(sensorNumber){
  case 1:
  {
    lbg.drawValue(sensorVal_1, graphMax);
    lcd.setCursor(0, 1);
    lcd.print("Sensor 1");
    break;
  }
  case 2:
  {
    lbg.drawValue(sensorVal_2, graphMax);
    lcd.setCursor(0, 1);
    lcd.print("Sensor 2");
    break;
  }
  case 3:
  {
    lbg.drawValue(sensorVal_3, graphMax);
    lcd.setCursor(0, 1);
    lcd.print("Sensor 3");
    break;
  }
  }
}

void hand_open()
```

```
{
    finger1.write(ext_a1);
    finger2.write(ext_a2);
    finger3.write(ext_a3);
    finger4.write(ext_a4);
    finger5.write(ext_a5);
}

void hand_close()
{
    finger1.write(flex_a1);
    finger2.write(flex_a2);
    finger3.write(flex_a3);
    finger4.write(flex_a4);
    finger5.write(flex_a5);
}

void set_threshold(int smin, int &st)
{
    st = smin+(graphMax-smin)/3;
}

void set_threshold_index(int smin, int &st)
{
    st = smin+(graphMax-smin)/2;
}

void reg_open()
{
    switch(index)
    {
        case 0:
            hand_open();
            break;
        case 1:
            finger1.write(ext_a1);
            break;
        case 2:
            finger2.write(ext_a2);
            break;
        case 3:
            finger3.write(ext_a3);
            break;
        case 4:
            finger4.write(ext_a4);
```

```
        break;
    case 5:
        finger5.write(ext_a5);
        break;
    }
}

void reg_close()
{
    switch(index)
    {
    case 0:
        hand_close();
        break;
    case 1:
        finger1.write(flex_a1);
        break;
    case 2:
        finger2.write(flex_a2);
        break;
    case 3:
        finger3.write(flex_a3);
        break;
    case 4:
        finger4.write(flex_a4);
        break;
    case 5:
        finger5.write(flex_a5);
        break;
    }
}

void forceFB_close()
{
    switch(index)
    {
    case 0:
        sweep_ALL_servos();
        break;
    case 1:
        sweep_servo(finger1, flex_a1, ext_a1);
        break;
    case 2:
        sweep_servo(finger2, flex_a2, ext_a2);
        break;
    }
```

```

case 3:
  sweep_servo(finger3, flex_a3, ext_a3);
  break;
case 4:
  sweep_servo(finger4, flex_a4, ext_a4);
  break;
case 5:
  sweep_servo(finger5, flex_a5, ext_a5);
  break;
}
}

void sweep_servo(Servo &myServo, int flex_angle, int ext_angle)
{
  int increment;
  long timeOfLastPos = 0;
  if (flex_angle > ext_angle) {
    increment = 1;
  }
  else {
    increment = -1;
  }
  int pos = ext_angle;
  while(pos != flex_angle)
  {
    if (millis()-timeOfLastPos > PosSweepDelay)
    {
      myServo.write(pos); // goes from ext_angle to flex_angle in steps of size "increment"
      timeOfLastPos = millis();
      pos += increment;
      timeOfLastSweep = millis();
      FSR1 = analogRead(A8); // read sensor data within sweep loop
      FSR2 = analogRead(A9);
      if (FSR1 > FSR_val || FSR2 > FSR_val)
      {
        break;
      }
    }
  }
}

void sweep_ALL_servos()
{
  long timeOfLastPos = 0;
  int pos1 = ext_a1;
  int pos2 = ext_a2;

```

```

int pos3 = ext_a3;
int pos4 = ext_a4;
int pos5 = ext_a5;
while(pos1 > flex_a1 || pos2 > flex_a2 || pos3 < flex_a3 || pos4 > flex_a4 || pos5 <
flex_a5)
{
  if (millis()-timeOfLastPos > PosSweepDelay)
  {
    finger1.write(pos1);
    finger2.write(pos2);
    finger3.write(pos3);
    finger4.write(pos4);
    finger5.write(pos5);
    timeOfLastPos = millis();
    pos1 -= 1;
    pos2 -= 1;
    pos3 += 1;
    pos4 -= 1;
    pos5 += 1;
    timeOfLastSweep = millis();
    FSR1 = analogRead(A8); // read sensor data within sweep loop
    FSR2 = analogRead(A9);
    if (FSR1 > FSR_val || FSR2 > FSR_val)
    {
      break;
    }
  }
}
}
}

```

## References

- [1] “New beBionic hand almost doubles its grip-strength, steered by user’s electrical ‘skin signals’.”[Online]. Available: <http://www.engadget.com/2012/09/07/bebionic-3-bionic-hand/>. [Accessed: 04-Dec-2012].
- [2] K. Nazarpour, A. H. Al-Timemy, G. Bugmann, and A. Jackson, “A note on the probability distribution function of the surface electromyogram signal.,” *Brain research bulletin*, pp. 10–13, Oct. 2012.
- [3] “Advancer Technologies.” [Online]. Available: <http://www.advancertechnologies.com/>. [Accessed: 29-Nov-2012].